

GHz reflectometry fingerprint imaging using epitaxial PbTiO₃ ultrasonic transducers

GHz 帯 PbTiO₃ エピ薄膜を用いた基板裏面での
反射率測定によるイメージング

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1. Introduction

Fingerprint reader based on PZT and ScAlN pMUT in the MHz range are extensively studied. In contrast, fingerprint imaging using thickness extensional mode AlN transducers in the GHz range were reported to improve spatial resolution [1]. However, the capacitive impedance of the AlN transducer become much higher than 50 Ω when size of the acoustic source is reduced, because of low dielectric constant of AlN.

In this study, to obtain small acoustic source with 50 Ω impedance matching, we reports epitaxial PbTiO₃ (PTO) transducer which possess high dielectric constant and electromechanical coupling coefficient k_t^2 . Moreover, we propose insertion loss imaging using time domain analysis of network analyzer.

Here, fingerprint imaging with 9 PbTiO₃ transducer array are demonstrated.

2. Fabrication of PbTiO₃ transducer array

PbTiO₃ epitaxial films were grown on a conductive La-SrTiO₃ substrate by RF magnetron sputtering. The crystalline orientation of the PbTiO₃ film was examined by X-ray diffraction (PANalytical, X'pert pro). PbTiO₃(002) peaks were observed in 2θ - ω XRD patterns as shown Fig. 1.

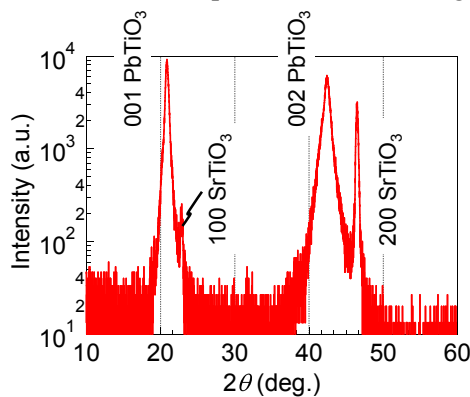


Fig. 1 XRD patterns of PbTiO₃ epitaxial film

3. Conversion loss of PbTiO₃ transducer

Electromechanical coupling coefficient k_t^2 of PbTiO₃ epitaxial transducers was estimated from longitudinal wave conversion loss curves which was measured by a network analyzer (Keysight Technologies, E9031C) [3,4]. Fig. 2 shows experimental conversion loss curves of PbTiO₃ epitaxial transducers. Minimum conversion loss was 2.2 dB at 0.8 GHz. Also, described are the theoretical curves simulated by Mason's equivalent circuit model. The theoretical curves agreed well with the experimental curves. k_t^2 of PbTiO₃ was demonstrated to be 28.9%.

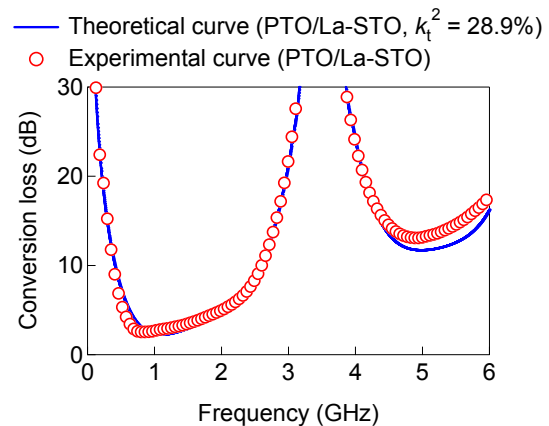


Fig. 2 Conversion loss of PbTiO₃ transducer

4. Insertion loss with and without elastomer

The thermoplastic elastomer was used as a substitute for the fingerprint. The difference of acoustic impedance between the substrate and the elastomer was smaller than that between the substrate and air. Insertion loss of piezoelectric film/substrate structure was degraded by contacting the elastomer due to the change of reflection coefficient of the substrate bottom/elastomer interface. Transducer insertion loss with and without elastomer were measured by a network analyzer. The maximum insertion loss with elastomer was 60%. On the other hand, maximum insertion loss without elastomer was 55%. The difference of reflection coefficient between with and without elastomer are confirmed.

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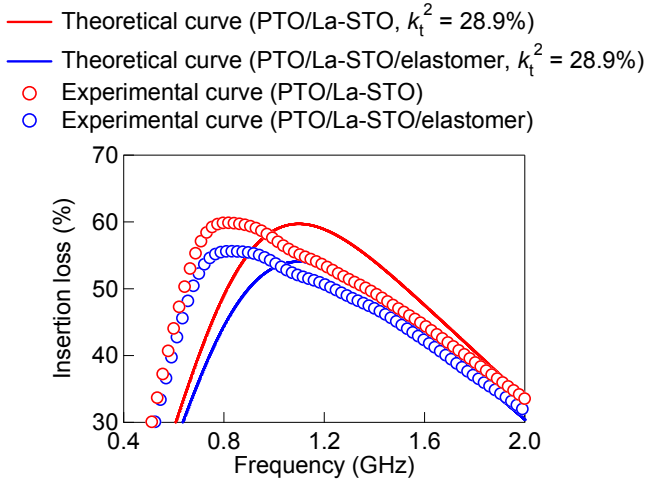


Fig. 3 Insertion loss curves of PbTiO₃ transducer with and without elastomer

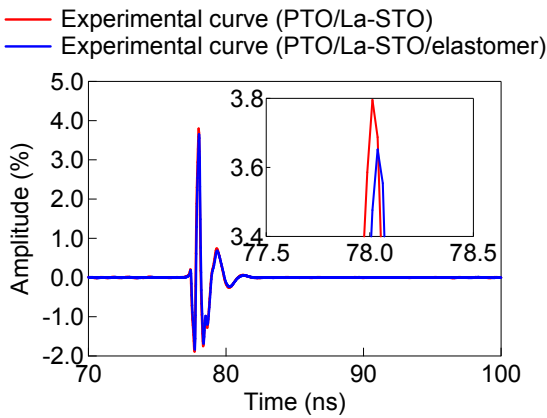


Fig. 4 Time domain impulse response of PbTiO₃ transducer with and without elastomer

4. Fingerprint imaging

The fingerprint elastomer phantom was contacted on the bottom of PbTiO₃ transducers. The maximum insertion loss images were obtained by mechanically scanning 9 PbTiO₃ transducer array. Fig. 6 shows the optical microscope image. Fig. 7 shows the acoustic maximum insertion loss image. Fig.8 shows the maximum first echo amplitude image.

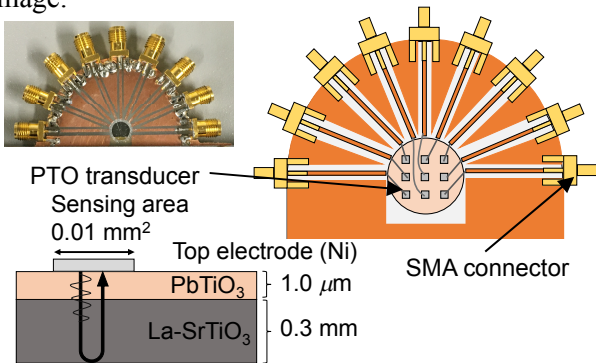


Fig.5 9 PbTiO₃ transducer array bonded the SMA connector and top electrode

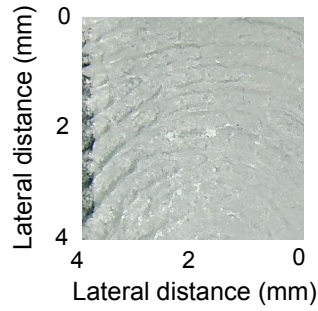


Fig. 6 Fingerprint phantom based on elastomer

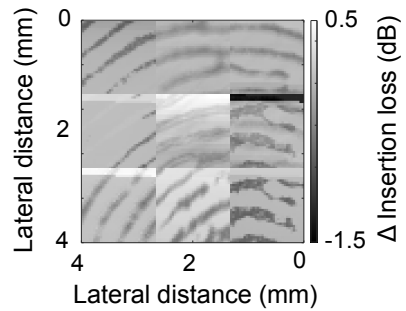


Fig.7 Maximum insertion loss image

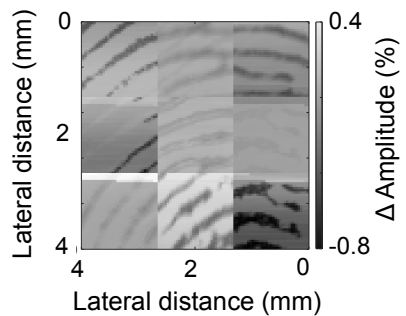


Fig.8 Maximum first echo amplitude image

5. Conclusion

PbTiO₃ epitaxial films were grown on conductive La-SrTiO₃ substrate. Electromechanical coupling coefficient k_t^2 of PbTiO₃ epitaxial transducers was 28.9%. We demonstrated phantom fingerprint imaging using 9 PbTiO₃ transducer array.

Acknowledgment

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